



SPECIFICATION

TITLE

"METHOD TO CORRECT THE B_1 FIELD IN MR MEASUREMENTS AND MR APPARATUS FOR IMPLEMENTING THE METHOD"

BACKGROUND OF THE INVENTION

Field of the Invention

The present invention concerns a method to correct the field strength of radio-frequency pulses, which in a magnetic resonance MR examination are emitted by an antenna of a magnetic resonance examination apparatus.

Description of the Prior Art

Magnetic resonance tomography is an increasingly employed technique to acquire images of the inside of the body of a living examination subject. In order to acquire an image with this modality, the body or a body part of the examination subject must first be exposed to as homogenous a static basic magnetic field as possible, which is generated by a basic field magnet of the magnetic resonance measurement device. During the data acquisition for the magnetic resonance images, rapidly switched gradient fields for spatial coding, which are generated by gradient coils, are superimposed on this basic magnetic field. Radio-frequency pulses of a defined field strength are then emitted into the examination subject with a radio-frequency antenna. The magnetic flux density of these radio-frequency pulses is typically designated as B_1 , the pulsed radio-frequency field is generally also called a B_1 field for short. By means of the radio-frequency pulses, in the examination subject magnetic resonance signals are excited which are acquired by a radio-frequency reception antenna. The reception antenna can either be the same antenna with which the radio-frequency pulses are emitted or a separate reception antenna. The magnetic resonance images of the examination subject are then

generated on the basis of the received magnetic resonance signals. A small physical volume, known as a "voxel," is associated with each image point in the magnetic resonance image. Each brightness or intensity value of the image points is linked with the signal amplitude of the magnetic resonance signal received from the voxel. The strength of the magnetic resonance signal is also dependent on, among other things, the strength of the emitted B1 field. Oscillations in the field strength of the excited B1 field thus lead to unintentional changes in the received magnetic resonance signal that can falsify the measurement result.

Typically, multiple transmission antennas are employed in magnetic resonance imaging as resonant antennas. Such antennas are differently energized by different loads, which, given constant feed power, leads to radio-frequency field strengths of different amplitudes. The load affecting the antenna is substantially dependent on, among other thing, the position of the examination subject in relationship to the antenna. Consequently, a new positioning of the patient between two magnetic resonance measurements within an examination, or an accidental movement of the patient, inevitably lead to a change of the antenna load and thus, given the same feed power, to a change of the B1 field. For this reason, a new adjustment of the transmitting power is typically implemented with each new positioning of a patient, in order to again set the B1 field to the correct value. Such an adjustment measurement is relatively complicated. As a rule, for this purpose the transmitting power is modified until, given a predetermined duration of the transmission pulse, by the influence of a radio-frequency pulse a specific, precisely measurable flip angle is set between the nuclear magnetization and the homogeneous magnetic basic field. Given the known flip angle and known pulse duration, the actual B₁ field that exists given the appertaining transmitting power is

determined. As a rule, the adjustment (calibration) ensues at a flip angle α of 180° , meaning at a location in which the nuclear magnetization is opposite to the static magnetic field, since in this case no magnetic field component exists transverse to the magnetic basic field. This transverse magnetization can be easily directly verified by the signal (free induction decay, FID) induced in the radio-frequency coil after the end of the exciting radio-frequency pulse. Therefore, to adjust the B_1 field, only the transmitting power must be varied, until the received FID signal is equal to zero.

A problem with this method is that, given multiple examinations, in particular given whole-body scans (such as, for example, in examinations in which blood vessels should be shown from the center of the body to the legs, using contrast), a faster measurement process is imperative. For such measurements to be implemented quickly, complicated transmitting power adjustments in the case of a new positioning of the patient can not be implemented for reasons of time. The adjustments are therefore often foregone at the cost of image quality.

SUMMARY OF THE INVENTION

It is an object of the present invention to provide a correction method and a magnetic resonance apparatus with which the field strength of the radio-frequency pulses, meaning the B_1 field, can be held substantially constant during an examination, even without the aforementioned adjustment measurements.

This object is achieved in a method and wherein the current flowing in the antenna for the transmission of a radio-frequency pulse is regulated by variation, by a predetermined nominal value, of the electrical power fed into the antenna. Use is made of the fact that the change of the load on the antenna effects a corresponding change of the loss resistance (equivalent resistance) of the antenna. This would

lead to a corresponding change of the current, without a correction of the feed power. In contrast, the B_1 field is always proportional to the current, independent of the load. This means, to a very good approximation, that a constant current in the transmitting antenna is synonymous with a constant B_1 field. By the regulation of the current by a predetermined nominal value by a corresponding correction of the feed power, a correspondingly constant B_1 field is emitted in a simple manner.

Given a table movement during the examination, the necessary feed power therefore need not be corrected by means of a corresponding magnetic resonance procedure, as was previously typical. Instead, a dynamic correction directly ensues by regulation of the current. This correction proceeds not in an independent sequence, but parallel to the running data acquisition without extending the measurement time. For a given patient position, a basic adjustment of the feed power merely must be implemented before the beginning of the actual data acquisition for imaging. In addition to the adjustment method described above, every other suitable method can be used.

In a simplified embodiment of the inventive method, the current is held at a constant value during the entire magnetic resonance examination. This means the current that was set in the basic adjustment of the feed power before the beginning of the actual examination is used as a nominal value. Such a regulation of the current by a constant value can be implemented relatively simply.

Given high frequencies of, for example, over 50 MHz, the field strength inside of the body is additionally independently modified by eddy currents and dielectric displacement currents. These effects can not be corrected by a simple regulation of the antenna current by a constant value. However, such currents ensuing in the examination subject during the measurement are dependent on the physical volume

in the field in a manner similar to the antenna load itself. In a preferred embodiment, the current changes in the antenna that ensue during the magnetic resonance examination are therefore under- or overcompensated in the regulation by a specific degree, in order to at least partially compensate during the examination, the influence of the currents within the examination subject on the field strength of the radio-frequency pulses. This is possible by varying the nominal value dependent on the currently determined actual current value, which is a measure for the load of the antenna. For this, for example, the nominal value can be raised or lowered by a specific empirically determined factor, dependent on the currently determined actual value. To determine such compensation factors, before the examination a number of test series can be implemented with different examination subjects or test persons. After the compensation factors are established once, a relatively good compensation of the additional currents ensuing in the examination subject is possible in a relatively simple manner with the inventive method.

In a further exemplary embodiment, the regulation of the current ensues phase-sensitively, meaning not only the amplitude is regulated, but also the phase of the current. In this manner, changes of the resonance frequency of the antenna caused by the patient, for example, by accidental approach of body parts to the antenna, can be compensated. Since phase changes in the B_1 field during a measurement would falsify the results, such a phase-sensitive regulation of the current or, respectively, B_1 field is sensible, in particular in a functional magnetic resonance imaging (fMRI) with which information about the activities in human and animal organs is be acquired, and consequently in which in particular changes of the received magnetic resonance signal must be evaluated.

To regulate the current by a nominal value, it is merely necessary to determine a proportionally appropriate restorative quantity and to supply this to a regulation device that appropriately varies the power fed to the antenna. There are various possibilities to determine an appropriate restorative quantity.

In a preferred embodiment, a number of field probes are used that are arranged in proximity to the antenna and, on the output side, are connected with the regulation device. In these field probes, a current is induced, dependent on the field emitted by the antenna, which is proportional to the field and thus to the current in the antenna. This voltages induced in the field proves are transmitted to the regulation device as output signals. "In proximity to the antenna", means that the field probes are located in the transmission area of the antenna, i.e. near enough to the antenna so that a sufficiently high voltage signal is induced in the probes. The field probes can be located outsides or inside of the volume encompassed by the antenna.

In principle, a single field probe can be used to determine the restorative quantity. However, at least two field probes, appropriately arranged at the antenna at a specific angle to one another, are preferably used in order to determine both linear polarized components of a circular polarized field emitted by the antenna. The field probes preferably are connected by a phase shifter with the regulation device that superimposes the output signals of the field probes, forming a mutual restorative signal. The phase shifting of the output signal of the field probes must be chosen dependent on the angle arrangements of the field probes to one another. Given use of two field probes which are disposed at a 90° angle to one another, this means the output signals must be correspondingly merged with a 90° phase shifter, and, for

example given a use of three probes which are each disposed at an angle of 120° to one another, a 120° phase shifter would have to be used, and so forth.

The use of at least two probes for both linear polarized components is sensible given circular polarized transmitting antennas, in order to be able to determine the variation in the circularity and the influence connected thereto on the necessary transmission amplitude.

Since the body geometry of a person to be examined is differentiated most strongly in the horizontal and vertical axes, and thus these directions represent different loads, the field probes are preferably arranged at an angle of 0° , 90° , 180° and/or 270° with regard to a horizontal slice plane through the person to be examined. The field probes preferably are mounted outside of the antenna, in order to prevent the probe feed lines from intersecting with the antenna structures.

In a further exemplary embodiment, the restorative signal for the current regulation is determined using directional couplers arranged in the antenna supply lines. Given an antenna with only one supply line, only one directional coupler is necessary. Given an antenna with a number of supply lines and a corresponding number of directional coupler, the directional couplers are, on the output side, respectively connected again with appropriate phase shifters, such that the decoupled signals of the directional coupler are appropriately superimposed with a phase-shift relative to one another. With such a directional coupler connected in the transmission path, the in-fed and the reflected voltages at the antenna are detected. The relationships at the feed point of the antenna thus are indirectly detected by a transformation on the power. Since the inductance, dependent solely on the antenna geometry, remains constant during the examination, the voltage induced in the directional coupler is proportional to the current in the antenna, and consequently

it can be obtained directly from the induced voltage signal of the directional coupler on the currents in the antenna.

DESCRIPTION OF THE DRAWINGS

Figure 1 is a basic block diagram of a circuit for supplying an antenna of an inventive magnetic resonance examination apparatus with radio-frequency pulses, with a regulation device according to a first exemplary embodiment.

Figure 2 is a basic block diagram of a circuit for supplying an antenna of an inventive magnetic resonance examination apparatus with radio-frequency pulses, with a regulation device according to a second exemplary embodiment.

Figure 3 is a basic block diagram of a circuit for supplying an antenna of an inventive magnetic resonance examination apparatus with radio-frequency pulses, with a regulation device according to a third exemplary embodiment.

Figure 4 is a basic block diagram of a circuit for supplying an antenna of an inventive magnetic resonance examination apparatus with radio-frequency pulses, with a regulation device according to a fourth exemplary embodiment.

DESCRIPTION OF THE PREFERRED EMBODIMENTS

In all exemplary embodiments, it is assumed that the antenna 1 is a transmission antenna 1 of a type known as a "birdcage antenna", typically used in magnetic resonance examination devices. These antenna 1 is assembled so as to resemble a birdcage and has a cylindrical shape with two end rings 3 at the ends and longitudinal rods 2 proceeding in parallel between the end rings 3. Capacitive elements are connected in the end rings 3 between the rods 2. With such an antenna 1, relatively homogenous circular polarized B_1 fields proceeding transverse to the cylinder axis A of the antenna 1 can be generated.

During an examination, a patient P is positioned along the cylinder axis A of the antenna 1 in the internal chamber of the antenna 1. The position of the patient P along the cylinder axis A can be changed between two individual exposures, in order to examine different body regions of the patient P. For this, the patient P is typically located on an examination bed (not shown) arranged within a plane E that can be moved in the direction of the cylinder axis A. The load of the antenna 1 is automatically changed by the change of the position of the patient P, and thus the antenna 1 is differently energized.

If a constant power were to be fed into the antenna 1 via the input lines 12, 13, the current I flowing in the antenna 1, and thus the field strength (i.e. the magnetic flux density of the radio-frequency pulses that are emitted by the antenna 1), would also change with the variation of the loading. In order to prevent this, in the exemplary embodiments of the invention, the current I in the antenna 1 is regulated by variation of the transmitting power by a constant value.

For this, in the exemplary embodiment according to Figure 1, a restorative signal RS is determined by means of two field probes (also called pickup probes) which is proportional to the current I flowing in the antenna 1. These field probes 4, 5 in this embodiment are mounted outside of the antenna 1 in proximity to the end rings 3. This has the advantage that the probe supply lines do not intersect the antenna structures. In principle, however, the field probes 4, 5 can also be arranged near the rods 2.

Upon emitting the radio-frequency pulses by the antenna 1, a voltage is induced in the probes 4, 5 which is proportional to the current I in the antenna 1. Both probes 4, 5 are arranged at 90° to one another at the (in Figure 1) forward end ring 3 of the antenna, such that both output signals S_1 , S_2 of both probes 4, 5,

meaning the induced voltages, are respectively proportional to the linear polarized components of the overall circular polarized field emitted by the antenna 1. Both output signals S_1 , S_2 are superimposed on one another by means of a 90° phase shifter and thus form a common restorative signal RS.

This restorative signal RS is converted (transformed) in a demodulator 10 into a direct voltage signal. The direct voltage signal is then compared within a comparator 11 with a reference signal or reference value FS which finally forms a nominal value, corresponding to the restorative signal RS, for the current I to be adjusted. A regulation difference is then present at the output of the comparator 11, which is linked via an amplitude modulator 8 with the incoming radio-frequency control signal HF. The radio-frequency control signal HF is influenced in the appropriate direction, such that the power fed into the antenna 1 is changed such that the current I remains constant in the antenna 1. The radio-frequency control signal HF output from the amplitude modulator 8 is amplified before the antenna 1 in a typical manner with an radio-frequency power amplifier 7 and split via a 90° coupler (90° hybrid) 6, such that two radio-frequency signals, phase-shifted 90° relative to one another, are appropriately fed into the antenna 1 via the antenna supply lines 12, 13, in order to generate overall a circular polarized B_1 field.

The modulation of the output signals S_1 , S_2 or the common restorative signal RS coming from the probes 4, 5, the comparison with the reference signal FS, and the correction of the transmission signal can ensue with analog and/or digital means.

Figure 2 shows modified exemplary embodiment of the circuit according to Figure 1. The representation of the antenna 1 and the examination subject P have been foregone here. The antenna 1 can be fashioned identical to the exemplary embodiment according to Figure 1.

In contrast to the exemplary embodiment according to Figure 1, however, here two field probes 4, 5 are used to determine a restorative signal. Instead, directional couplers 14, 15 are connected in the antenna supply lines 12, 13 which respectively decouple a signal S_{3a} , S_{3b} , S_{4a} , S_{4b} from the wave propagating forward and back on the appertaining antenna supply line 12, 13. The decoupling signals S_{3a} , S_{3b} , S_{4a} , S_{4b} of the directional couplers 14, 15 corresponding to the wave running forward and back are respectively added in adders 16, 17. Before this the signals S_{3a} , S_{4a} corresponding to the back-propagating wave are phase-shifted in phase shifters 18, 19 by an angle that directly compensates the phase shifting that the signal experienced from the directional coupler to the antenna and back. Both the transmit times on the connection cables and the phase shifts in the antenna adaptation network contribute to this. Signals S_3 , S_4 then exist at the output of the respective adders 16, 17 that are proportional to the voltage at the associated in-feed point of the appertaining supply line 12, 14 at the antenna 1. Both signals S_3 , S_4 are then coupled with one another via a 90° phase shifter, and thus form a restorative signal RS' to regulate the current I of the antenna 1 at a constant value. The further processing of this restorative signal RS' ensues analogously to the exemplary embodiment in Figure 1. Likewise, the influence of the radio-frequency control signal HF ensues in the same manner, dependent on the restorative signal RS' .

Figure 3 shows a variant in which not only the amplitude, but also the phase of the current I is evaluated and considered in the regulation. With such a regulation, changes of the antenna resonance frequency effected by the patient can also be compensated. Such antenna resonance frequency changes can ensue, for

example, by the patient positioned within the antenna 1 moving, for example, a hand moving closer to the antenna 1.

In the exemplary embodiment according to Figure 3, it is assumed that the restorative signal RS is determined by probes 4, 5 arranged at the antenna 1, as in the exemplary embodiment according to Figure 1. The output signals S_1 , S_2 from the probes 4, 5 are first superimposed on one another via a 90° phase shifter 9 to form a common restorative signal RS.

This restorative signal RS already contains the information as to the amplitude and the phase of the current I. The restorative signal RS is therefore split and on is supplied to a demodulator 10, as in the exemplary embodiment according to Figure 1, such that from this a direct voltage signal is generated that is compared with the reference value FS in the comparator 11. In a typical manner, the output signal of the comparator 11 therefore is used in order to influence the radio-frequency control signal HF in a suitable manner by an amplitude modulator 8.

Additionally, the restorative signal RS is given to an input of a phase comparator 22 in which the restorative signal RS is compared with the phase of the arriving radio-frequency control signal HF. The difference signal is then supplied to the input of a regulator 21 that has a phase shifter 20 that is arranged between the amplitude modulator 8 and the power intensifier 7 in the supply line for the resource file control signal HF to the antenna 1. In this phase shifter 20, the difference signal is then modified corresponding to the phase of the input radio-frequency control signal HF in the correct manner, in order to compensate the change of the antenna resonance frequency and the phase change in the antenna 1 as a consequence thereof.

Figure 4 shows a further exemplary embodiment that is arranged substantially as the exemplary embodiment according to Figure 3. The signal difference between the two exemplary embodiments is that here the reference signal FS is also generated from the radio-frequency control signal HF itself. For this, the part of the radio-frequency control signal HF decoupled for the phase comparator 22 is also supplied to a rectifier, which rectifies the radio-frequency control signal HF and, on the output side, generates the desired guide signal FS for the comparator 11. The radio-frequency control signal HF to be fed in is particularly well suited as an amplitude nominal value, since it is a very precise signal that exactly exhibits the pulse shape necessary for the emission of the correct radio-frequency pulses.

Instead of a birdcage antenna another antenna shape can be used. Likewise, in a simple exemplary embodiment only a single probe can be used in order to generate a restorative signal, or a larger number of probes can be used. A combination of the various exemplary embodiments is also possible, for example a decoupling of the restorative signal with one or more directional couplers and a subsequent phase-sensitive regulation.

Although modifications and changes may be suggested by those skilled in the art, it is the intention of the inventors to embody within the patent warranted hereon all changes and modifications as reasonably and properly come within the scope of their contribution to the art.